Reduced Sleep Spindles and Spindle Coherence in Schizophrenia: Mechanisms of Impaired Memory Consolidation?


Background: Sleep spindles are thought to induce synaptic changes and thereby contribute to memory consolidation during sleep. Patients with schizophrenia show dramatic reductions of both spindles and sleep-dependent memory consolidation, which may be causally related.

Methods: To examine the relations of sleep spindle activity to sleep-dependent consolidation of motor procedural memory, 21 chronic, medicated schizophrenia outpatients and 17 healthy volunteers underwent polysomnography on two consecutive nights. On the second night, participants were trained on the finger-tapping motor sequence task (MST) at bedtime and tested the following morning. The number, density, frequency, duration, amplitude, spectral content, and coherence of stage 2 sleep spindles were compared between groups and examined in relation to overnight changes in MST performance.

Results: Patients failed to show overnight improvement on the MST and differed significantly from control participants who did improve. Patients also exhibited marked reductions in the density (reduced 38% relative to control participants), number (reduced 36%), and coherence (reduced 19%) of sleep spindles but showed no abnormalities in the morphology of individual spindles or of sleep architecture. In patients, reduced spindle number and density predicted less overnight improvement on the MST. In addition, reduced amplitude and sigma power of individual spindles correlated with greater severity of positive symptoms.

Conclusions: The observed sleep spindle abnormalities implicate thalamocortical network dysfunction in schizophrenia. In addition, the findings suggest that abnormal spindle generation impairs sleep-dependent memory consolidation in schizophrenia, contributes to positive symptoms, and is a promising novel target for the treatment of cognitive deficits in schizophrenia.

Key Words: Memory consolidation, motor skill, procedural learning, schizophrenia, sleep, sleep spindles

Sleep disturbances in schizophrenia have been described since Kraepelin (1) and are a common complaint throughout its course (2), including in the prodrome (3), but the nature of the abnormalities and their relations to the pathophysiology, cognitive deficits, and symptoms of schizophrenia remain poorly understood (4). Several recent studies have reported markedly reduced sleep spindle activity in schizophrenia (5–8). Mediated by thalamocortical circuits, spindles are a defining feature of stage 2 non-rapid eye movement (NREM) sleep, evident in the electroencephalogram (EEG) as brief bursts of 12 Hz to 15 Hz synchronous activity. Animal studies point to spindles as a key mechanism of synaptic plasticity, mediating memory consolidation during sleep (9–12). In humans, spindles correlate with overnight memory consolidation across diverse learning paradigms (13). In schizophrenia, memory deficits are a key neurocognitive abnormality and there is evidence of impaired consolidation across multiple domains (14–16). In particular, schizophrenia patients have marked impairments of sleep-dependent motor procedural memory consolidation (17) in the context of reduced spindle activity (5,8). We conducted a new study to more completely specify the nature of sleep spindle abnormalities in schizophrenia and their relation to deficient sleep-dependent memory consolidation.

The most widely reported sleep architecture abnormalities in schizophrenia—reduced slow wave sleep (18–20) and abnormal rapid eye movement sleep (20–22)—are not consistently observed and have not withstood meta-analyses (23,24). Relatively few studies have gone beyond sleep architecture to examine the EEG spectral characteristics of sleep. Three older studies of unmedicated patients that identified NREM spindles with visual detection at a single EEG channel had contradictory findings. Poulin et al. (20) examined spindles in the 12 Hz to 14 Hz range and found no differences between patients (n = 11) and control participants. Van Cauter (25) also reported no differences in patients (n = 9) compared with control participants. Finally, Hiatt et al. (26) found that patients (n = 5) showed increased spindle density during a 10-minute NREM segment but did not distinguish between stage 2 and slow wave sleep across participants. In contrast, several recent studies that used automated spindle detection algorithms, a larger number of EEG channels, and larger samples comprised of chronic medicated schizophrenia patients report a dramatic reduction of sleep spindles (5–8). In one of these studies, the spindle deficit was associated with greater severity of positive symptoms and was absent in a nonschizophrenic psychotic control group treated with antipsychotic medications (7), suggesting that the spindle deficit influences symptom presentation and is not due to treatment with antipsychotic medications. To characterize the functional significance of the sleep spindle deficit in schizophrenia, we examined the relations of spindle activity to overnight consolidation of motor memory and to symptoms.
We employed the same simple, well-characterized test of motor procedural learning used in our previous studies of schizophrenia, the finger tapping motor sequence task (MST) (27,28). After training on the MST, healthy young participants show significant improvement in speed after a night of sleep but not after an equivalent period of wake (28). In young healthy individuals, overnight improvement on the MST and other simple motor skill tasks correlates with the amount of stage 2 sleep (28) and with the number and density of sleep spindles (29–32). In two studies, we have reported that this overnight improvement is absent in schizophrenia (5,17). Our primary hypothesis was that reduced stage 2 sleep spindle activity would correlate with impaired overnight memory consolidation in schizophrenia. We also expected patients to show reduced spindle coherence during sleep based on evidence of reduced EEG coherence during quiet awake (33–36) and dysconnectivity in thalamocortical networks in schizophrenia (37–39).

**Methods and Materials**

**Participants**

Twenty-five schizophrenia outpatients were recruited from an urban mental health center and 21 completed the study. Patients had been maintained on stable doses of atypical antipsychotic medications for at least 6 weeks and 12 took diverse adjunctive medications for anxiety, agitation, and/or concurrent mood disturbance (Table S1 in Supplement 1). Diagnoses were confirmed with Structured Clinical Interviews for DSM-IV (40) and symptoms were rated with the Positive and Negative Syndrome Scale (PANSS) (41).

Twenty-one healthy control participants, screened to exclude a personal history of mental illness, family history of schizophrenia spectrum disorder, and psychoactive medication use, were recruited from the community by poster and website advertisements and 18 completed the study.

All participants were screened to exclude diagnosed sleep disorders, treatment with sleep medications, a history of significant head injury, neurological illness, and substance abuse or dependence within the past 6 months. One control participant was excluded for sleeping less than 4 hours on two of the five nights preceding the laboratory visit based on wrist actigraphy and sleep log data. The final sample of 21 schizophrenia and 17 control participants did not differ in age, sex, or parental education (Table S2 in Supplement 1). All participants gave written informed consent. The study was approved by the Institutional Review Boards of Massachusetts General Hospital, the Massachusetts Department of Mental Health, and Beth Israel Deaconess Medical Center.

**Procedures**

In the week before their stay in the Clinical Research Center (CRC), participants completed informed consent, demographic questionnaires, and rating scales; toured the CRC; and received an actigraph to wear until study completion. Participants also completed home sleep logs.

Participants spent 2 consecutive weeknights in the CRC with standard montage including five to eight channels of EEG (F3, F4, C3, Cz, C4, Pz, O1, O2) referenced to the linked mastoids, electromyography, and electro-oculography. Data from all available electrodes were analyzed for each participant.

**Finger Tapping Motor Sequence Task.** The MST involves pressing four numerically labeled keys on a standard computer keyboard with the fingers of the left hand, repeating a five-element sequence (4-1-3-2-4) “as quickly and accurately as possible” for 30 seconds. The numeric sequence was displayed at the top of the screen, and dots appeared beneath it with each keystroke. During both training and test sessions, participants alternated tapping and resting for 30 seconds for a total of 12 tapping trials. The primary outcome measure was the number of correct sequences per trial, which reflects both the speed and accuracy of performance. Practice-dependent improvement was defined as the percent increase in correct sequences from the first training trial to the average of the last three training trials. Overnight improvement was calculated as the percent increase in correct sequences from the last three training trials to the first three test trials the following morning (27).

**Actigraphy.** The Mini-Mitter Actiwatch-64 (Philips Respironics, Bend, Oregon) records wrist movement in 15-second epochs to provide estimates of sleep time based on periods of wrist immobility. Standard scoring algorithms were used to determine time in bed (TIB), total sleep time (TST), and sleep efficiency (TST/TIB).

**Sleep Architecture.** Each 30-second epoch of PSG sleep was visually classified into stages (wake, 1, 2, 3, 4, and rapid eye movement) according to standard criteria (42) by raters blind to diagnosis and night. Awakenings were scored when one or more 30-second epoch was classified as wake following initial sleep onset. Sleep stages are reported as the percentage of TST.

**Spindle Analyses.** We analyzed spindles during stage 2 sleep, given our primary hypothesis of a relation of stage 2 sleep spindles with memory consolidation. Polysomnography data were preprocessed and analyzed using BrainVision Analyzer 2.0 (BrainProducts, Munich, Germany) and MatLab R2009b (The MathWorks, Natick, Massachusetts). Artifacts were automatically detected and removed and EEG data were filtered at .5 Hz to 35 Hz. Artifact rejection was confirmed by visual inspection.

Power spectral density (μV²/Hz) was calculated by Fast Fourier Transform (FFT), applying a Hanning window to successive 3-second epochs of stage 2 sleep with 50% overlap. Sigma band (12–15 Hz) spectral power, which correlates with sleep spindle activity, was divided into low (12–13.5 Hz) and high (13.5–15 Hz) sigma band power (43,44).

Discrete sleep spindle events were automatically detected using a wavelet-based algorithm. The raw EEG signal was subjected to a time-frequency transformation using an 8-parameter complex Morlet wavelet (45). Spindles were detected at each EEG channel by applying a thresholding algorithm to the extracted wavelet spectrum corresponding approximately to the 10 Hz to 16 Hz frequency range. For thresholding, the rectified moving average of the signal was first calculated, using a 100-millisecond sliding window. A spindle event was identified whenever this wavelet signal exceeded threshold (defined as 4.5 times the mean signal amplitude of all artifact-free epochs) for a minimum of 400 milliseconds. This method was validated by examining the correlation of algorithmically detected spindle density with hand-counted spindles in 10
control participants \((r = .87; \text{slope} = 1.2 \text{ automated/hand scored})\) and 10 patients \((r = .95; \text{slope} = 1.8)\). The ratio of algorithm-detected to hand-counted spindles was not significantly different between groups. As spindle density is known to correlate with sigma power, albeit moderately since background sigma-frequency EEG activity weakens the correlation \((43)\), we also correlated algorithm-detected spindle density with 12 Hz to 15 Hz sigma power in all control participants \((r = .50, p = .04)\) and patients \((r = .52, p = .02)\).

For each spindle, measures of amplitude, sigma power, duration, and peak frequency were based on analysis of 2-second EEG epochs centered on the point of spindle detection (Figure 1). Within the sigma range \((12–15 \text{ Hz})\), amplitude was the maximal voltage following 12 Hz to 15 Hz band pass filtering; peak frequency was defined as the spectral peak of the spindle following FFT decomposition; and sigma power was defined as the mean FFT-derived power spectral density across the 12 Hz to 15 Hz range \((\mu \text{V}^2/\text{Hz})\) (Figure 1B).

To examine the time-frequency characteristics of individual spindles, wavelet analysis was conducted at Cz, where detected spindles were most numerous in both control and patient samples. A complex Morlet wavelet was applied separately to each spindle epoch (Figure 1, right). The duration of each spindle was calculated as the half-height width of wavelet energy within the spindle frequency range. Finally, we assessed the cross-spectrum/auto-spectrum sigma coherence \((46)\) of spindles across EEG channels. Coherence \((\text{Coh})\) of spindles across EEG channels \((c)\) was assessed for each 2-second epoch during which a spindle was auto-detected in any channel. Coherence values range from 0 to 1, calculated as the cross-spectrum \((\text{Coh})\)/auto-spectrum coherence within the full 12 Hz to 15 Hz sigma frequency band \((f)\), according to the formula:

\[
\text{Coh}(c_1, c_2)(f) = |\text{Coh}(c_1, c_2)(f)|^2 / (|\text{Coh}(c_1, c_1)(f)| |\text{Coh}(c_2, c_2)(f)|)
\]

**Results**

**Sleep Architecture**

Patients and control participants showed relatively normal sleep and did not differ significantly on any measure of sleep quality or architecture measured either as the total number of minutes or the percentage of TST spent in any sleep stage during the experimental nights (Table 1). Actigraphy indicated that patients spent significantly more TIB and had more TST during the prestudy nights.

**Spindle Number, Density, and Sigma Power**

Relative to control participants, schizophrenia patients exhibited markedly reduced hand-sleep spindle number \((36\% \text{ reduction})\) and density \((38\%)\) (Figure 2A, left; Table 1) \((p = .01\) for all electrodes). While control participants showed a typical spindle-frequency peak in the stage 2 power spectrum, this peak was dramatically reduced in the patient group (Figure 2C). Sigma power was significantly reduced in patients in the low-frequency but not high-frequency sigma band (Table 1). There were no group differences in the delta \((1–4 \text{ Hz})\), theta \((4–7 \text{ Hz})\), alpha \((8–12 \text{ Hz})\), or beta \((13–25 \text{ Hz})\) frequency bands (Figure 2D). The reductions in sigma power were more pronounced when calculated relative to the overall EEG power baseline (Figure 2C, Table 1).

### Table 1. Sleep Data in Patients and Control Participants Reported as Means ± SD

<table>
<thead>
<tr>
<th></th>
<th>Patients ((n = 21))</th>
<th>Control Participants ((n = 17))</th>
<th>(p)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Sleep Architecture</td>
<td></td>
<td></td>
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<tr>
<td>TST (minutes)</td>
<td>443 ± 79</td>
<td>413 ± 55</td>
<td>.19</td>
</tr>
<tr>
<td>Stage 1 %</td>
<td>9 ± 6</td>
<td>9 ± 1</td>
<td>.76</td>
</tr>
<tr>
<td>Stage 2 %</td>
<td>54 ± 10</td>
<td>56 ± 7</td>
<td>.40</td>
</tr>
<tr>
<td>SWS %</td>
<td>17 ± 10</td>
<td>13 ± 5</td>
<td>.12</td>
</tr>
<tr>
<td>REM %</td>
<td>19 ± 4</td>
<td>22 ± 7</td>
<td>.17</td>
</tr>
<tr>
<td>WASO (minutes)</td>
<td>70 ± 60</td>
<td>61 ± 46</td>
<td>.62</td>
</tr>
<tr>
<td>Awakenings/hour</td>
<td>4.1 ± 2.5</td>
<td>4.2 ± 1.5</td>
<td>.86</td>
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<td>Spindle Measures</td>
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<td></td>
<td></td>
</tr>
<tr>
<td>Spindle number</td>
<td>308 ± 144</td>
<td>485 ± 122</td>
<td>.0003*</td>
</tr>
<tr>
<td>Spindle density/minute</td>
<td>1.3 ± .5</td>
<td>2.1 ± .6</td>
<td>.0001*</td>
</tr>
<tr>
<td>Low sigma power ((\mu \text{V}^2/\text{Hz}))</td>
<td>.043 ± .02</td>
<td>.074 ± .06</td>
<td>.03*</td>
</tr>
<tr>
<td>High sigma power ((\mu \text{V}^2/\text{Hz}))</td>
<td>.034 ± .02</td>
<td>.043 ± .03</td>
<td>.27</td>
</tr>
<tr>
<td>Characteristics of Individual Spindles</td>
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<td>-</td>
<td>-</td>
</tr>
<tr>
<td>Amplitude ((\mu \text{V}))</td>
<td>16.8 ± 3.4</td>
<td>17.3 ± 5.0</td>
<td>.67</td>
</tr>
<tr>
<td>Frequency (Hz)</td>
<td>12.9 ± 1.5</td>
<td>13.0 ± 1.8</td>
<td>.50</td>
</tr>
<tr>
<td>Duration (seconds)</td>
<td>1.01 ± 1.6</td>
<td>1.04 ± 0.5</td>
<td>.47</td>
</tr>
<tr>
<td>Sigma power ((\mu \text{V}^2/\text{Hz}))</td>
<td>.31 ± .13</td>
<td>.35 ± .19</td>
<td>.51</td>
</tr>
<tr>
<td>Sigma coherence (0–1)</td>
<td>.35 ± .09</td>
<td>.43 ± .10</td>
<td>.02*</td>
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<tr>
<td>Prestudy Actigraphy</td>
<td></td>
<td></td>
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</tr>
<tr>
<td>TIB (minutes)</td>
<td>589 ± 96</td>
<td>454 ± 73</td>
<td>.0003*</td>
</tr>
<tr>
<td>TST (minutes)</td>
<td>521 ± 99</td>
<td>402 ± 70.6</td>
<td>.0004*</td>
</tr>
<tr>
<td>Sleep efficiency %</td>
<td>88 ± 5</td>
<td>88 ± 5</td>
<td>.80</td>
</tr>
</tbody>
</table>

REM, rapid eye movement; SD, standard deviation; SWS, slow wave sleep; TIB, time in bed; TST, total sleep time; WASO, wake after sleep onset.

*Significance at \(p < .05\).

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**Figure 1.** Frequency and time-frequency decomposition of individual spindle events used to define amplitude, frequency, and duration variables. (A) Electroencephalogram trace of a sleep spindle waveform filtered at 12 Hz to 15 Hz, (B) Fast Fourier Transform of the same sleep spindle, and (C) wavelet decomposition of the spindle, representing spectral power across time. Spindle duration defined as half-height width of wavelet energy.
participants showed significant overnight improvement. During training (63% vs. 58%, and control participants did not differ in the amount of learning curves on day 1 and the failure of overnight improvement with standard error bars. Right: topographical map of reduced sigma coherence of spindles in schizophrenia across electrodes. Solid lines indicate electrode pairs showing a significant reduction in schizophrenia following correction for multiple comparisons (p < .0006); dashed lines indicate significance at the uncorrected p < .05 level. (C) Spectral power in control participants (heavy line) and patients (light line) at the Cz electrode, where sigma power was maximal. The sigma band baseline (12–15 Hz, dashed line) is a best fit to the 11 Hz to 12 Hz and 15 Hz to 16 Hz data. (D) Logarithm of spectral power across the broader 0 Hz to 25 Hz range at the Cz electrode. There were no group differences in the delta (1–4 Hz), theta (4–7 Hz), alpha (8–12 Hz), or beta (13–25 Hz) frequency bands. Spectral profiles were similar across all recording sites.

![Image](image.png)

**Figure 2.** Spindle activity. (A) Bar graph of sleep spindle density during stage 2 sleep averaged across electrode sites with standard error bars. (B) Left: bar graph of sigma-band coherence during spindles averaged across electrode sites with standard error bars. Right: topographical map of reduced sigma coherence of spindles in schizophrenia across electrodes. Solid lines indicate electrode pairs showing a significant reduction in schizophrenia following correction for multiple comparisons (p < .0006); dashed lines indicate significance at the uncorrected p < .05 level. (C) Spectral power in control participants (heavy line) and patients (light line) at the Cz electrode, where sigma power was maximal. The sigma band baseline (12–15 Hz, dashed line) is a best fit to the 11 Hz to 12 Hz and 15 Hz to 16 Hz data. (D) Logarithm of spectral power across the broader 0 Hz to 25 Hz range at the Cz electrode. There were no group differences in the delta (1–4 Hz), theta (4–7 Hz), alpha (8–12 Hz), or beta (13–25 Hz) frequency bands. Spectral profiles were similar across all recording sites.

### Morphology of Individual Spindles

There were no significant differences in the characteristics of individual spindles between groups. The average amplitude, duration, and peak frequency of individual spindles differed by less than 3% between groups, and the average sigma power in individual spindles differed by 12% (Table 1). The distribution of spindles across the scalp was also similar in patients and control participants, with the greatest number of spindles detected at central recording sites for both groups.

**Spindle Coherence**

Patients showed reduced cross-electrode coherence of individual spindles in the sigma band (19% reduction relative to control participants) (Figure 2B; Table 1), with several individual electrode pairs surviving Bonferroni correction based on eight electrode sites (Cz-C3, Cz-O1, Cz-F3, and C3-O2; mean 33% reduction for these sites, all ps < .006).

In schizophrenia, overnight improvement correlated with both spindle number [r(21) = .46, p = .04] and density [r(21) = .45, p = .04] (Figure 4). In contrast, control participants showed no correlation with spindle number [r(17) = -.09, p = .73] and a trend toward a negative correlation between spindle density and overnight improvement [r(17) = -.43, p = .09] that was primarily driven by a single outlier whose value exceeded the 75th percentile by greater than 1.5 times the interquartile range in a boxplot analysis (outlier excluded; r(16) = -.23, p = .40). The correlations of spindle number and density with overnight MST improvement were significantly stronger in patients [group by spindle: number F(2,35) = 4.00, p = .03; density without outlier F(2,34) = 3.50, p = .04]. MST improve-

![Image](image.png)

**Figure 3.** Overnight improvement on the motor sequence task (MST) in patients and control participants. (A) Bar graphs of overnight improvement with standard error bars. (B) Motor skill learning across training and the first three test trials for control participants (triangles) and schizophrenia (SZ) patients (circles). The y axis is scaled separately for control participants (left) and patients (right) to highlight the qualitative similarity of learning curves on day 1 and the failure of overnight improvement in the schizophrenia group only. The dashed line is the regression line fit to data from the last six training trials. The discontinuity in the x axis represents a night of sleep. Patients and control participants did not differ in the amount of learning during training (63% vs. 58%, p = .77), but only control participants showed significant overnight improvement.
ment was not related to sigma coherence of spindles in either group. Correlations of MST improvement with spindle parameters were similar on both nights, and the change in spindle parameters from the baseline to the testing night did not correlate with MST improvement.

Relations of Spindles to Symptoms

Lower peak amplitude \( r(211) = -0.47, p = 0.03 \) and sigma power \( r(211) = -0.45, p = 0.04 \) of individual spindles correlated with greater severity of positive but not negative symptoms. No other measure of spindle activity correlated with positive or negative symptoms.

Medication Effects

Neither chlorpromazine equivalent nor illness duration correlated with any measure of spindle activity. Spindle densities in participants divided by medication type are presented in Table S1 in Supplement 1. Participants taking clozapine \((n = 9)\) exhibited significantly lower spindle densities than other patients \( t(19) = 2.60, p = 0.02 \). When these patients were excluded from analysis, the remaining patients still exhibited lower spindle number \( t(27) = 2.86, p = 0.008 \) and density \( t(27) = 2.89, p = 0.008 \) than control participants. No other medication type significantly affected spindle parameters.

Discussion

The present study is the first to demonstrate a relationship between sleep spindle activity and sleep-dependent memory consolidation in schizophrenia. Relative to control participants, schizophrenia patients showed fewer sleep spindles, a lower density of sleep spindles, and less overnight improvement on the MST than control participants. Within the schizophrenia group, spindle number and density both predicted overnight MST improvement. Although the present study cannot establish causality, these findings are consistent with the hypothesis that reduced spindle activity impairs memory consolidation in schizophrenia. We also report, for the first time, reduced spindle coherence across the cortex in patients compared with control participants, suggesting that there is reduced synchrony in thalamocortical spindle-generating networks in schizophrenia. This resonates with the large body of literature showing reduced EEG coherence, particularly in the beta and gamma bands, during wake in schizophrenia (for review, see [47]) and extends these observations to sleep. Finally, the amplitude and power of individual sleep spindles were inversely related to positive symptoms in schizophrenia. These findings suggest that abnormal sleep spindles contribute to cognitive deficits and symptoms in schizophrenia and offer a novel biomarker and target for treatment development.

The hypothesis that sleep spindle abnormalities contribute to cognitive deficits in schizophrenia is consistent with mounting evidence concerning the function of spindles (13). In healthy individuals, spindles are thought to promote synaptic plasticity critical to memory consolidation during sleep (12), thus mediating the overnight consolidation of both declarative and procedural memory (29–51), and to index learning potential and general intelligence (52,53). In this context, we note that spindles are also reported to be abnormal in several other neurodevelopmental disorders affecting cognition, including mental retardation (54), phenylketonuria (55), and autism (56).

Sleep spindles are generated in the thalamic reticular nucleus (TRN) (57), which is comprised entirely of gamma-aminobutyric acid (GABA)ergic neurons (58). Thalamic reticular nucleus neurons primarily project to glutamatergic thalamic neurons that then project to the cortex. Cortical neurons, in turn, send glutamatergic inputs back to N-methyl-D-aspartate acid (NMDA) receptors on TRN neurons. Thus, spindles are mediated by a thalamocortical feedback loop that is regulated by both GABAergic and NMDA-receptor mediated glutamatergic neurotransmission (59). The TRN is thought to be the spindle pacemaker, as TRN neurons exhibit spindle frequency burst firing in vivo (60,61), which is believed to rhythmically entrain thalamocortical relay neurons and ultimately the cortex (62). While the TRN can generate spindles in isolation (63,64), glutamatergic feedback from the cortex is critical for the synchronization of spindles (43,65). As sleep spindles are temporally correlated with hippocampal sharp-wave ripples (10,11), coherent expression of spindles across wide areas of cortex could reflect the synchronous reactivation of recent memory traces across cortical regions. Such reactivation is thought to mediate the consolidation of newly acquired information into more permanent forms for long-term storage and integration (66,67). In schizophrenia, reduced and less synchronous spindle activity because of thalamocortical dys-function could interfere with sleep-dependent memory processing by preventing the simultaneous reactivation of memory compo-
ments stored across visual, spatial, emotional, and goal-representa-
tion networks, thus leading to a fragmentation of memory and
cognition.

While the exact mechanism of spindle deficits in schizophrenia
is unknown, the reduction in spindle activity may reflect thalamic
dysfunction, while decreased spindle synchrony may reflect abnor-
nal NMDA receptor-mediated thalamic responses to cortical in-
puts. This hypothesis is consistent with evidence of GABA deficits
(68) and abnormal expression of NMDA receptors and glutamate
transporters in the thalamus in schizophrenia (69,70). In this con-
text, it is striking that current models of schizophrenia posit dys-
function in thalamocortical circuitry and in both GABA and the
NMDA glutamatergic systems. Future studies using GABA and/or
NMDA receptor agonists could provide greater insight into the
mechanisms underlying spindle abnormalities in schizophrenia
and their contribution to impaired sleep-dependent memory.

A limitation to the interpretation of our findings is that the
patients were treated with a variety of second generation antipsy-
chotics and adjunctive agents and we did not have adequate power
to examine the effects of different medication types on our out-
come measures. For example, the four patients who took benzodi-
azepines, which are known to increase sleep spindles and sigma
power (e.g., [71,72]), did not differ from other patients on spindle
parameters. While a prior study of schizophrenia reported de-
creased sleep spindle activity following a single dose of olanzapine
(73), the effects of chronic atypical antipsychotic treatment on spin-
dle activity are unknown. In the present study, the subset of pa-
tients taking clozapine showed significantly fewer spindles, but the
spindle reduction remained significant in those patients not taking
clozapine, and it is unclear whether the more profound reduction
reflects the medication itself or illness factors that lead to treatment
with clozapine. Moreover, antipsychotic dosage was not related to
any measure of spindle activity. The recent finding of a spindle
deficit in schizophrenia, but not in a nonschizophrenic psychiatric
control group treated with antipsychotic medications, suggests
that the deficit is unlikely to be merely a side effect of antipsychotics
(7). While the present study cannot exclude a contribution from
medications, even if the spindle reductions were affected by med-
ications, illness progression, or epiphenomena of long-term illness,
since the vast majority of patients with schizophrenia are chronic
and medicated, the findings remain clinically important.

There are discrepancies with prior work that merit consider-
ation. While our findings of reduced spindle number and density in
schizophrenia agree with those of Ferrarelli et al. (6,7), we observed
these reductions across all electrode sites and did not see reduc-
tions in spindle amplitude and duration, suggesting that spindles
are morphologically similar in patients and control participants.
Differences in spindle detection algorithms may account for these
discrepancies. We also note that in the present study the spindle
parameters that were inversely correlated with positive symptoms,
the amplitude and sigma power of individual spindles, were not
abnormal in schizophrenia and that our findings differ from Fer-
arelli et al. (7), who found inverse correlations of integrated spindle
activity and spindle number with positive symptoms. The present
sample had only mild symptoms (PANSS total = 55 ± 7) and was
less symptomatic than the sample of Ferrarelli et al. (7) (PANSS
total = 89, variability not provided). The restricted range and mild
symptoms of the present sample may limit the generalizability of our
findings. Larger, more heterogeneous samples may be necessary to
determine which positive symptoms correlate with specific spindle
parameters, as this may provide clues to the mechanisms of these
relations.

Unlike some previous studies (e.g., [32,74]), we did not detect
any effects of motor task training on spindle characteristics in either
group. Spindle parameters did not differ significantly on the base-
line and testing nights and the changes in spindle activity did not
correlate with overnight MST improvement. These findings are
more consistent with evidence that the EEG power spectrum dur-
ing NREM sleep in humans is relatively stable over time, resistant to
experimental perturbations, and genetically mediated (75,76).

Although our prior study failed to detect a significant correlation
between spindle density and overnight MST improvement in schizophre-
nia (5), the effect size was remarkably similar [r(14) = .46,
 \( p = .10 \) prior study; r(21) = .45, \( p = .04 \) here] and the difference in
significance reflects that the sample was smaller by a third. Related
to this, unlike some previous studies of the MST in young healthy
control participants (29,31), spindle activity did not correlate with
overnight improvement in the middle-aged healthy control partic-
ipants of either the present or prior study. We are not aware of any
studies that show correlations in middle-aged participants and a
recent study of older adults (mean age 68) found significant over-
night MST improvement but no correlation of improvement with
any measure of spindle power (rs range from \(-.07\) to \(.06\) [77]). In
addition, the more restricted range of both spindle activity and
overnight improvement in control participants compared with pa-
tients in the present study may have limited our ability to detect a

Figure 5. Overnight improvement as a function of spin-
dle density and number in all participants combined,
with the best fit nonlinear saturating function lines. MST,
motor sequence task.
correlation. When control participants and patients are plotted together, the relations between spindle density and number with overnight improvement are best described by saturating nonlinear inverse functions [density: \( R^2(36) = 20, \ p = .005; \) number: \( R^2(36) = .24, \ p = .002; \) Figure 5], suggesting that spindle activity improves MST performance but only up to a point beyond which further increases do not lead to additional benefit.

In summary, we report that reduced sleep spindle activity predicts impaired consolidation of motor procedural memory and increased severity of positive symptoms in schizophrenia, suggesting that disrupted thalamocortical activity during stage 2 sleep contributes to both cognitive deficits and symptoms. Reduced and less synchronized spindle activity may impair memory consolidation by interfering with normal processes of coordinated memory reactivation and consolidation during sleep. We therefore propose that abnormal sleep spindles be considered as a potentially treatable contributor to cognitive deficits in schizophrenia.

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